GLCM based Improved Mammogram Classification using Associative Classifier

Jyoti Deshmukh and Udhav Bhosle
Rajiv Gandhi Institute of Technology, Andheri (w), Mumbai-400053
University of Mumbai, INDIA
Email: {jyoti.deshmukh, udhav.bhosle}@mctrgit.ac.in

Abstract—Among women, 12% possibility of developing a breast cancer and 3.5% possibility of mortality due to this cause is reported [1]. Nowadays early detection of breast cancer became very important. Mammogram - a breast X-ray is used to investigate and diagnose breast cancer. In this paper, authors propose GLCM (Grey Level Co-occurrence Matrix) feature based improved mammogram classification using an associative classifier. Mining of association rules from mammogram dataset discovers frequently occurring patterns. It depends on user specified minimum confidence and support value. This dependency causes an increase in search space. The authors propose two-phase optimization procedure to overcome these limitations.

The initial phase comprises feature optimization by adopting proposed PreARM (Pre-processing step for Association Rule Mining) method. The next phase comprises association rule optimization by adopting proposed ESAR (Extraction of Strong Association Rules) method to generate efficient, highly correlated and robust rules. Proposed associative classification method is substantiated by adapting authentic MIAS and DDSM mammogram database. The experimentation concedes 91% and 90% trimming of GLCM features and association rules by adopting PreARM and ESAR algorithms respectively. Using optimized association rules, the classification accuracies procured for MIAS and DDSM datasets are 92% and 94% respectively. Area under Receiver Operating Characteristic (ROC) curves obtained by proposed system for MIAS and DDSM datasets are 0.9656 and 0.9285 respectively. Results of GLCM based associative classifier are compared with GLCM based Random Forest (RF), an ensemble learning method. The experimental result shows that GLCM based associative classifier outperforms RF method with respect to accuracy and AUC, and it is a promising method for mammogram classification.

Index Terms—Mammogram, ROI, GLCM, PreARM, Apriori algorithm, ESAR.

I. INTRODUCTION

Globally the numbers of woman’s carcinoma cases are gradually increasing. As the cause of the breast cancer is still not clearly identified, so its early prevention is not possible. Hence there is a need of early identification of carcinoma to improve the survival scale. In the available methods, mammography proved to be a superior diagnostic procedure for the prior identification of carcinoma, due to its reliability, cost-effectiveness and less radiation-dosage [1]. Medical survey presents that death rate due to breast cancer can be lowered by more than 30% with the help of mammographic screening [2]. It is also discovered that, only 30% of patients, that experienced biopsy after the mammographic screening, have actual cancerous mass [3]. It means many patients have suffered the pain of unwanted biopsy, which happened because of incorrect diagnosis of masses. Hence, computerized diagnosis of mammograms is the necessity for radiologists and physicians to enhance diagnosis accuracy.

Thus, classification of masses into cancerous or non-cancerous has become important issue for the early diagnosis. Many methods are proposed by the researchers to categorize mammograms into cancerous or non-cancerous. From large collection of mammograms, image mining system automatically finds the meaningful information or knowledge. In [4] authors introduce mining concepts on image datasets to extract the knowledge. They focus on process of extracting the association rules from color images. In [5], approach of identifying frequent pattern using association rules is explained. In [6] Ramani et al. discussed pre-processing techniques for mammograms.

In [7], process of automatic segmentation of breast image is carried out to detect its area of concern, with the help of region growing technique. Relation in feature discrimination power and feature vector dimension is described in [8]. Increase in the count of features, causes increase in data dimensionality. As a result, it causes reduction in significance of each feature. Similar patterns are retrieved from a dataset, with the help of textural feature. Information about texture is obtained from spatial representation of pixel intensities, which characterizes texture information. In the proposed method, GLCM features are used to illustrate the mammogram texture information. As GLCM features carries semantically significant information about texture and it helps in the process of mammogram classification [9].

More often, available frequent pattern mining algorithms produce a large count of redundant association rules, which affects the mining performance. In [10] associative classification scheme is explained to improve
the classification accuracy of mammograms. Low-level mammogram texture features and radiologist’s viewpoint is used for frequent pattern searching. In [11], [12] and [13] authors present association rule based, effective diagnosis of mammograms. Authors used association rule mining approach for data-mining and Neural Networks as a classifier. A composition of association rules along with a rough set theory is used for computer aided diagnosis of mammogram images by Yun et al. [14]. In [15], authors conferred a classification method, build on weighted association rules.

In this paper, authors propose an algorithm to obtain significant and frequent patterns from mammogram dataset which are used for mammogram classification. Apriori algorithm is used to obtain association rules. However, all obtained rules are not useful. Many rules are redundant, and resulted in exponential search space. Authors propose two phase optimization scheme for obtaining strong and eminently correlated association rules. It comprises feature optimization using proposed PreARM algorithm followed by association rule optimization by applying ESAR algorithm.

The presented scheme is verified using authentic MIAS and DDSM mammogram dataset. Presented scheme works in four steps. The step one includes image segmentation, GLCM texture feature extraction and optimization of features using the PreARM algorithm. The second step is generation of transaction database, which is an input for Apriori algorithm to produce rules. In the third step, optimization of association rules to acquire robust rules using EASR algorithm. Classification of mammogram is carried out using strong and optimized rules in fourth step. Results are reported in terms of accuracy, specificity, sensitivity, recall, precision, and area under ROC.

The paper outline is described as below. Proposed scheme is explained in Section II followed by experimental results in Section III. Lastly, section IV describes conclusion and future work.

II. PROPOSED METHOD

Fig. 1 explains the proposed associative classification scheme’s flow diagram. Here the modernity is in optimization of feature space and corresponding association rules. Optimization step gives most discriminating features and strong rules, which helps to curtail search space and consequently enhances the classification accuracy. Pre-processing using histogram equalization, thresholding and contrast stretching is carried out on mammograms, and segmentation is performed to acquire region of interest of mammograms.

A. Mammogram feature extraction

GLCM method is used to extract the features from the segmented mammograms and they are organized in feature vectors. Relative frequency of occurrences of i and j pixels with distance d pixels, and 0 orientation is stated by a co-occurrence matrix \( M(d, 0) \). For 0°, 45°, 90°, and 135° directions, and 1, 2, 3, 4 and 5 distances co-occurrence matrices are determined. For each matrix seven features are determined. Each mammogram is presented with feature vector of size \([140 \times 1]^T\) [9]. Texture feature used are as follow

\[
\text{Step} = \sum_i \sum_j P(i, j) 
\]

\[
\text{Variance} = \sum_i \sum_j (i - j)^2 P(i, j) 
\]

Fig.1. Proposed associative classification scheme flow diagram
Entropy = \sum \sum P(i, j) \log(P(i, j)) \quad (3)

Energy = \sum \sum P(i - j)^2 \quad (4)

Homogeneity = \sum \sum \frac{P(i-j)}{1+|i-j|} \quad (5)

3rd Moment = \sum \sum P(i-j)^3 P(i,j) \quad (6)

Inverse Variance = \sum \sum \frac{P(i,j)}{(i-j)^2} \quad (7)

B. Feature optimization

Optimization of GLCM features is performed using PreARM algorithm [16]. Keyword of mammogram image (benign or malignant) and the feature vector are given as input to PreARM algorithm. Optimization and discretization of continuous GLCM features are carried out in this step. Exact number of intervals and features are chosen depending upon inconsistency in features.

Reduction in the number of feature value interval reduces the inconsistency in the features [10]. PreARM aims to have the most discriminative features to present the smallest class variation [16].

C. Transaction database and Association rule generation

Transaction database is prepared using optimized feature vectors and respective class labels of training mammogram images. Apriori algorithm produces association rules using transaction database. Consider T is the set of objects and R is set of data cases. Association rule is presented as U → V; U, V \subset T and U \bigcap V = \phi. Where U and V are antecedent and consequent part of association rule. Association rule is evaluated using its confidence and support value. These are defined as,

Support, S (U \rightarrow V) = P(U \bigcup V) \quad (8)

Confidence, C (U \rightarrow V) = P(V | U) \quad (9)

D. Association Rules optimization

Apriori algorithm generates all association rules which meet specified minimum criteria of support and confidence. More often, rules with high value of confidence and support give redundant information, which makes it weak rule. Values of confidence and support are inadequate to filter uninteresting rules. Likewise confidence and support, correlation measures are chosen to determine association rules as stated in [17]. Association rule is represented as

U \rightarrow V \{support, confidence, correlation measures\} \quad (10)

Here, lift, certainty factor and completeness correlation measures are preferred to obtain strong rules. These measures are presented as

Lift (A, B) = \frac{P(A \cup B)}{P(A)P(B)} \quad (11)

Completeness (A, B) = \frac{P(A \cup B)}{P(B)} \quad (12)

Certainty factor (A, B) = \max \left( \frac{P(A)}{1-P(B)}, \frac{P(B)}{1-P(A)} \right) \quad (13)

ESAR algorithm [18] is adopted to obtain optimized and strong rules. For individual rule confidence, support, lift, completeness and certainty factor values are calculated. The minimum threshold value of RCM (resultant correlation measure) is decided empirically. The rules satisfying RCM threshold are considered to be robust rules. Algorithm 1 presents ESAR algorithm.

Algorithm 1: ESAR algorithm

Input:  n: count of all association rules, value of Confidence, Support, Lift, Completeness and Certainty factor of every rule and minimum RCM threshold.

Output: Optimized association rules

1. Initialize S = 0
2. For every rule ri, and i ≤ n
3. Compute supp(ri), Conf(ri), C1(ri), C2(ri)
4. If Lift (ri) > 1
5. Then RCM(ri) = [supp(ri) * Conf(ri) * C1(ri) * C2(ri)]
6. If RCM(ri) > RCM threshold
7. S + +
8. End
9. Else RCM(ri) = [supp(ri) * Conf(ri) * C1(ri) * C2(ri)] / 4
10. If RCM (ri) > RCM threshold
11. S + +
12. End
13. End
14. End For

E. Classification of mammograms using Associative classifier

Algorithm 2 presents Associative classification algorithm [16]. The GLCM feature vector of the test image is derived by using feature extraction method and given to the classification step. In this step, test image is classified into cancerous or non cancerous class with the help of strong rules. Class labels present at the consequent portion of the rule are saved by associative classification algorithm. Test image feature vector is matched with the antecedent portion of all optimized rules. When GLCM feature value of the test image is present in the feature value interval of benign or malignant mammogram, count of benign (or malignant) class is increased respectively. Input test mammogram is classified to the class, which has the highest matches.
Algorithm 2: Associative classification algorithm

**Input:** All optimized rules, test mammogram’s feature vector

**Output:** Test mammogram class (benign or malignant)
1. Compare test mammogram’s feature vector with the antecedent portion of each rule (antecedent → consequent), where each class belongs to consequent portion.
2. If feature vector matches antecedent, and if consequent belongs to benign class (or malignant class), count of benign class (or malignant class) increases respectively.
3. Compare count of benign and malignant class.
4. Classify test image to the class having the highest count.

F. Classification of mammograms using Random Forest (RF) method

To improve the classification performance, different ensemble classification methods are used. In ensemble classification method, training of many classifiers is performed and their results are added along with voting for getting output of the ensemble classifier. RF is [19], [20] a composite classifier, constructed using a collection of tree classifiers. It is a meta learner, built using many individual trees. It works very fast on large databases. Trees used in RF are obtained using random samples; Training of individual tree in the forest is independent of other trees in the forest. So, RF is a good example of parallelization.

Bagging or boosting is used in RF classifier for developing ensemble of classifier with classification tree CART (Classification And Regression Tree). Majority vote of tree determine the output of the classifier. RF runs effectively on bigger datasets. In the proposed work, RF is used to classify mammograms and compared the results with associative classifier. Algorithm 3 presents classification of mammograms using RF method.

Algorithm 3: Classification using Random Forest method

**Input:** Optimized features of the training images with class

**Output:** Test image class (benign or malignant)
1. Consider N: Count of training images; M: Count of variables in the classifier; m: Count of input variables utilized for decision making at a node of tree and m is less than M
2. Randomly select m variables and use it for decision making at each node of tree.
3. Determine the superior split with the help of m variables during the training of mammogram data set.
4. Construct a forest for i=1 to N using a tree classifier (CART).
5. Select the training data set by random sampling with replacement.
6. Utilize the remaining data sets to validate the performance of the tree.

Tree Construction: Tree is completely grown without pruning.

III. EXPERIMENTAL RESULTS AND DISCUSSIONS

To corroborate the proposed method, the experiment is carried out in MATLAB environment. Mammograms from Mammography Image Analysis Society (MIAS) database [21] and Digital Data-base for Screening Mammography (DDSM) [22] are considered to verify proposed scheme. Experiments are carried out on 64 bit I5, 2.50 GHZ processor with 4 GB RAM. The count of abnormal mammograms used is listed in Table 1.

Fig. 2(a-e) shows outputs of segmentation process. Digitization noise induced in the course of mammogram acquisition is eliminated by applying median filtering during pre-processing step. Fig. 2(a) present input mammogram, fig. 2(b) shows median filtered mammogram. Empirically, a global threshold value is set to 100 to convert the input mammogram image into binary mammogram. Fig. 2(c) present output of thresholding process. To eliminate artifacts, wedges and labels morphological operations are performed on binary mammograms, followed by contrast enhancement technique. Fig. 2(d) present output mammogram of contrast enhancement technique. Region growing algorithm is applied to segment pectoral muscles of input mammogram, in which seed is located inside the pectoral muscles [7]. Fig. 2(e) present output of mammogram segmentation process with area of interest. Feature vector is generated using GLCM method for mammograms from MIAS and DDSM database. Out of 140 original features, 10 and 12 most discriminative features are obtained after optimization for every mammogram from DDSM and MIAS database respectively to form optimized feature vector.

In transaction database, a class of the image is listed in the column one and optimized feature value interval labels are listed in the rest of the columns. Apriori algorithm accepts transaction database as input to generate association rules. The parameters availed and the number of association rules generated for both the datasets by Apriori algorithm is presented in Table 2. Table 3 lists the sample association rules mined. Table 4, 5 and 6 lists the sample feature vector, optimized feature vector and transaction database for MIAS database. Optimized rules are obtained using EASR algorithm. Empirically, value of RCM is set to 0.02. All rules, accomplishing the RCM threshold criteria are determined as robust rules. Two phase optimization result i.e. feature and association rule optimization using PreARM and ESAR algorithm and result of mammogram classification obtained by proposed scheme are listed in Table 7.

<table>
<thead>
<tr>
<th>Database</th>
<th>Total Images</th>
<th>Training Images</th>
<th>Testing Images</th>
</tr>
</thead>
<tbody>
<tr>
<td>DDSM</td>
<td>320</td>
<td>288</td>
<td>32</td>
</tr>
<tr>
<td>MIAS</td>
<td>114</td>
<td>89</td>
<td>25</td>
</tr>
</tbody>
</table>

Table 1. Number of mammogram images used for classification from DDSM and MIAS database.

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Table 2. Parameters used and result of Apriori algorithm

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Number of rules</th>
</tr>
</thead>
<tbody>
<tr>
<td>Min-supp threshold</td>
<td>0.01</td>
</tr>
<tr>
<td>Min-conf threshold</td>
<td>0.50</td>
</tr>
<tr>
<td>MIAS</td>
<td>14232</td>
</tr>
<tr>
<td>DDSM</td>
<td>10289</td>
</tr>
</tbody>
</table>

Table 3. Sample association rules

<table>
<thead>
<tr>
<th>Association rule</th>
<th>Description</th>
</tr>
</thead>
<tbody>
<tr>
<td>R1: 35, 144 → 101</td>
<td>Mammogram with optimized feature value interval label 35 and 144 is benign.</td>
</tr>
<tr>
<td>R2: 3, 24, 86 → 102</td>
<td>Mammogram with optimized feature value interval label 3, 2 and 86 is malignant.</td>
</tr>
</tbody>
</table>

Figure 3 represents sample result of classification, figure 3(a) is test image classified as benign and figure 3(b) is test image classified as malignant. Accuracy measures used for the mammogram classification scheme are sensitivity, specificity, recall and precision. Table 8 presents performance measures values of the associative classifier for MIAS and DDSM database. The confusion matrix for MIAS and DDSM database is listed in Table 9. Performance of proposed GLCM based associative classifier is compared with RF method [19]. ROC curves of associative classifier and RF method for MIAS and DDSM database are shown in Fig. 4 and 5 respectively.

![Fig. 2. Results of segmentation process](image)

(a) (b) (c) (d) (e)

Table 4. Feature vector

<table>
<thead>
<tr>
<th>Image Number (1-89)</th>
<th>Features (1-140)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>1 2 3 4 ... 134 135 136 137 138 139 140</td>
</tr>
<tr>
<td>1</td>
<td>657 655 652 650 ... 2.91 3.07 3.05 3.08 3.13 3.16 3.13</td>
</tr>
<tr>
<td>2</td>
<td>657 655 652 650 ... 0.59 0.71 0.82 0.44 0.54 0.62 0.66</td>
</tr>
<tr>
<td>3</td>
<td>657 655 652 650 ... 0.93 1.07 1.15 0.74 1.13 1.5 1.89</td>
</tr>
<tr>
<td>4</td>
<td>657 655 652 650 ... 3.66 3.8 3.89 3.88 4.01 3.94 3.73</td>
</tr>
<tr>
<td>5</td>
<td>657 655 652 650 ... 5.73 6.27 6.67 4.16 5.25 6.02 6.54</td>
</tr>
<tr>
<td>6</td>
<td>650 647 645 642 ... 3.84 4.16 4.34 3.63 3.68 3.81 4.07</td>
</tr>
<tr>
<td>7</td>
<td>657 655 652 650 ... 5.27 5.89 6.35 3.56 4.74 5.43 6.09</td>
</tr>
<tr>
<td>8</td>
<td>657 655 652 650 ... 2.43 2.57 0 0 0 0 0</td>
</tr>
<tr>
<td>9</td>
<td>657 655 652 650 ... 2.96 3.28 1.19 0.48 0.6 0.64 0.65</td>
</tr>
<tr>
<td>10</td>
<td>657 655 652 650 ... 3.07 3.05 0 0 0 0 0</td>
</tr>
<tr>
<td></td>
<td>... ... ... ... ... ... ... ... ... ... ... ... ... ...</td>
</tr>
<tr>
<td>89</td>
<td>657 655 652 650 ... 4.88 5.35 3.32 4.49 5.08 5.28 4.37</td>
</tr>
</tbody>
</table>

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Table 5. Optimized feature vector

<table>
<thead>
<tr>
<th>Image Number (1-89)</th>
<th>12 Optimized Features (21-139)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>21</td>
</tr>
<tr>
<td>1</td>
<td>0.36</td>
</tr>
<tr>
<td>2</td>
<td>0.42</td>
</tr>
<tr>
<td>3</td>
<td>2.97</td>
</tr>
<tr>
<td>4</td>
<td>2.66</td>
</tr>
<tr>
<td>5</td>
<td>2.67</td>
</tr>
<tr>
<td>6</td>
<td>2.26</td>
</tr>
<tr>
<td>7</td>
<td>0.37</td>
</tr>
<tr>
<td>8</td>
<td>0.37</td>
</tr>
<tr>
<td>9</td>
<td>1.1</td>
</tr>
<tr>
<td>10</td>
<td>1.46</td>
</tr>
</tbody>
</table>

Table 6. Transaction database

<table>
<thead>
<tr>
<th>Image Class 101-Benign 102-Malignant</th>
<th>Optimized feature value interval label</th>
</tr>
</thead>
<tbody>
<tr>
<td>101</td>
<td>2  26  50  74  120  144  168  170  194  218  242  266</td>
</tr>
<tr>
<td>101</td>
<td>7  31  56  75  107  137  160  176  200  223  248  267</td>
</tr>
<tr>
<td>101</td>
<td>11 31  56  85  112  137  160  179  202  223  248  277</td>
</tr>
<tr>
<td>101</td>
<td>21 43  64  91  117  125  152  189  211  235  256  283</td>
</tr>
<tr>
<td>101</td>
<td>20 45  70  95  99  123  147  188  211  237  262  287</td>
</tr>
<tr>
<td>101</td>
<td>20 43  67  92  97  125  149  188  211  235  259  284</td>
</tr>
<tr>
<td>101</td>
<td>19 43  67  94  100 125  149  187  211  235  259  286</td>
</tr>
<tr>
<td>102</td>
<td>13 34  59  88  111 134  157  181  205  226  251  280</td>
</tr>
</tbody>
</table>

Table 7. Result of two phase optimization and mammogram classification

<table>
<thead>
<tr>
<th>Mammogram Database</th>
<th>GLCM features</th>
<th>Optimized features</th>
<th>Apriori algorithm Rules</th>
<th>Optimized rules</th>
<th>Accuracy</th>
</tr>
</thead>
<tbody>
<tr>
<td>MIAS</td>
<td>140</td>
<td>12</td>
<td>14232</td>
<td>1010</td>
<td>90.90%</td>
</tr>
<tr>
<td>DDSM</td>
<td>140</td>
<td>10</td>
<td>10280</td>
<td>1162</td>
<td>100%</td>
</tr>
</tbody>
</table>

Table 8. Performance measures of the associative classifier for MIAS and DDSM database

<table>
<thead>
<tr>
<th>Mammogram Database</th>
<th>Performance measure (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Sensitivity</td>
</tr>
<tr>
<td>MIAS</td>
<td>92.85</td>
</tr>
<tr>
<td>DDSM</td>
<td>87.5</td>
</tr>
</tbody>
</table>

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FPR (false positive rate) represents horizontal axis, TPR (true positive rate) represents vertical axis of ROC curve respectively.

\[
TPR = \frac{TP}{P} \quad (14)
\]

\[
FPR = \frac{FP}{N} \quad (15)
\]

If TP is obtained (i.e. a malignant mammogram classified as malignant), both TP and TPR increases. In ROC plot, moved up and plotted the point. FP is obtained (i.e. a benign mammogram classified as malignant), both FP and FPR increases. In ROC plot, moved right and plotted the point. Similar task is performed for every test mammogram, i.e. moved up direction for TP and towards the right for a FP [17]. If FN is obtained then TP decreases, so TPR decreases and hence it results in decrease in AUC value.

The maximum area under ROC curve values obtained by the proposed classifier and random forest method for MIAS database are 0.9656 and 0.8398, and for DDSM database are 0.9285 and 0.9270 respectively.

The authors propose the GLCM feature based improved mammogram classification using an associative classifier. Optimization of GLCM features and association rules is achieved using PreARM and ESAR algorithm respectively. Presented scheme is validated on MIAS and DDSM mammogram datasets.

Further the classification of mammogram images is carried out with the help of optimized association rules. Proposed technique gives better classification accuracy around 92% for MIAS and 94% for DDSM database as compared with the other associative classification techniques. Area under ROC curve value obtained by the proposed scheme for MIAS and DDSM database are 0.9656 and 0.9285 respectively. For comparative analysis, results of proposed GLCM based associative classifier are compared with GLCM based RF method. Experimental results reveal that suggested scheme gives better AUC and accuracy are two statistics measures and gives different qualities of the classifier. So AUC and accuracy of a classifier may not be consistent. Results are compared with the other associative classification techniques in terms of accuracy. For MIAS data set, result of BPNN (Back Propagation Neural Network) method is 81.25% [11], ARC-AC (Association Rule Based Classification with All Categories) method is 69.11% [12][13], ARC-BC (Association Rule Based Classification By Categories) method is 80.33% [12][13], JAC (Joining Associative Classifier) method is 77.49 [14], WAR-BC(Weighted Association Rule Based Classifier) method is 89.69% [15], and proposed associative classification method is 92% for MIAS and 94% for DDSM data set. It shows that, proposed approach of classification gives better accuracy compared with other methods reported in literature.

IV. CONCLUSIONS

Mammograms are low-dose X-ray images, used to investigate human breast. For radiologist, most challenging job is to find correct information from the mammograms, which is used for diagnosis process. The authors propose the GLCM feature based improved mammogram classification using an associative classifier.

Optimization of GLCM features and association rules is achieved using PreARM and ESAR algorithm respectively. Presented scheme is validated on MIAS and DDSM mammogram datasets.

Further the classification of mammogram images is carried out with the help of optimized association rules. Proposed technique gives better classification accuracy around 92% for MIAS and 94% for DDSM database as compared with the other associative classification techniques. Area under ROC curve value obtained by the proposed scheme for MIAS and DDSM database are 0.9656 and 0.9285 respectively. For comparative analysis, results of proposed GLCM based associative classifier are compared with GLCM based RF method. Experimental results reveal that suggested scheme gives better
performance over RF method. Proposed method is validated as a critical approach for the elimination of redundant and weak rules. Moreover, computation cost of mammogram analysis can be reduced, and it can be used for other image classification applications.

Fig.4. ROC curves for MIAS database

Fig.5. ROC curves for DDSM database

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**Authors’ Profiles**

**Jyoti Deshmukh** is Ph.D. Research Scholar, Department of Electronics and Telecommunication Engineering, Rajiv Gandhi Institute of Technology, Mumbai, and University of Mumbai, India. She received her B. Tech (Computer Science and Technology) from SNDT University, Mumbai in the year 2004 and ME (Computer Engineering) from University of Mumbai in 2008. She is working as Assistant Professor in the department of Computer Engineering, Rajiv Gandhi Institute of Technology, Mumbai, India.

**Udhav Bhosle** received his Ph.D. in Electrical Engineering, from Indian Institute of Technology, Mumbai in 2004. He received his BE (Electronics) and ME (Electronics and Telecommunication) from SGS Institute of Engineering and Technology, Nanded, an Autonomous Institute under Government of Maharashtra in the year 1989 and 1995 respectively. He is Principal and Professor Department of Electronics and Telecommunication Engineering, Rajiv Gandhi Institute of Technology, Mumbai, and University of Mumbai. His research interest includes Signal and Image processing, Computer Vision and Communication Engineering.

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